

Confocal Microscopy and Related Techniques

Chau-Hwang Lee (李超煌)

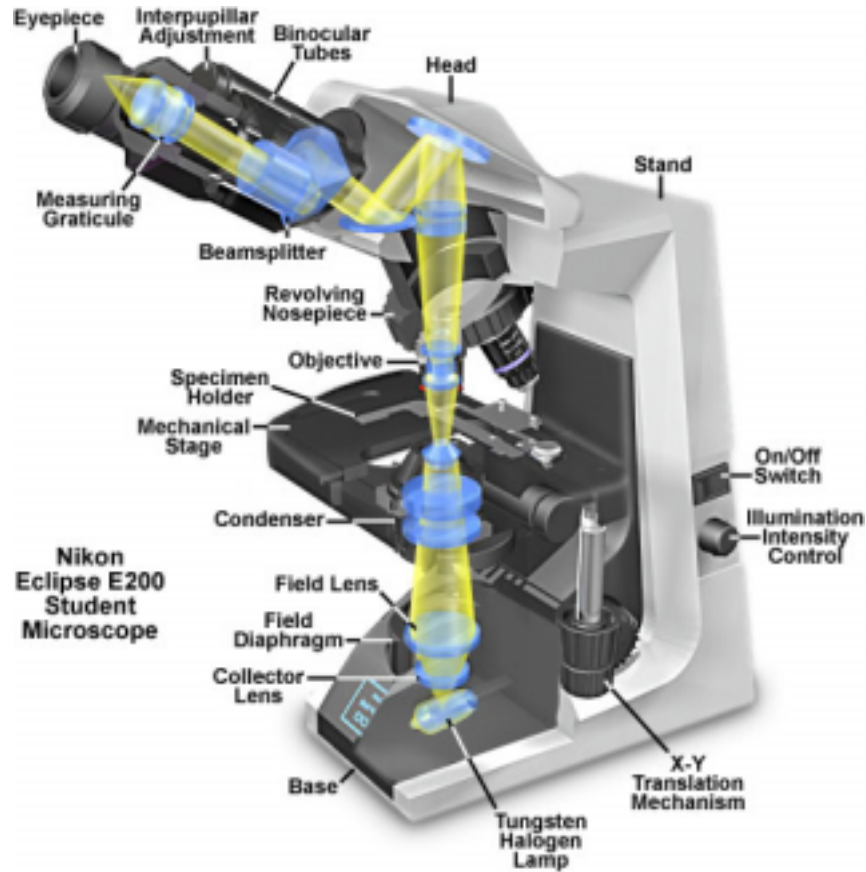
Associate Research Fellow

*Research Center for Applied Sciences, Academia Sinica
128 Sec. 2, Academia Rd., Nankang, Taipei 11529, Taiwan*

E-mail: clee@gate.sinica.edu.tw

Imaging Microscopy

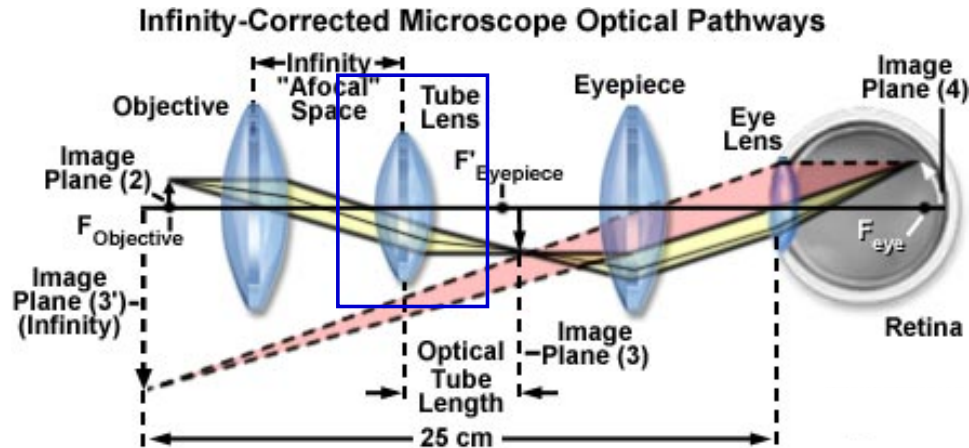
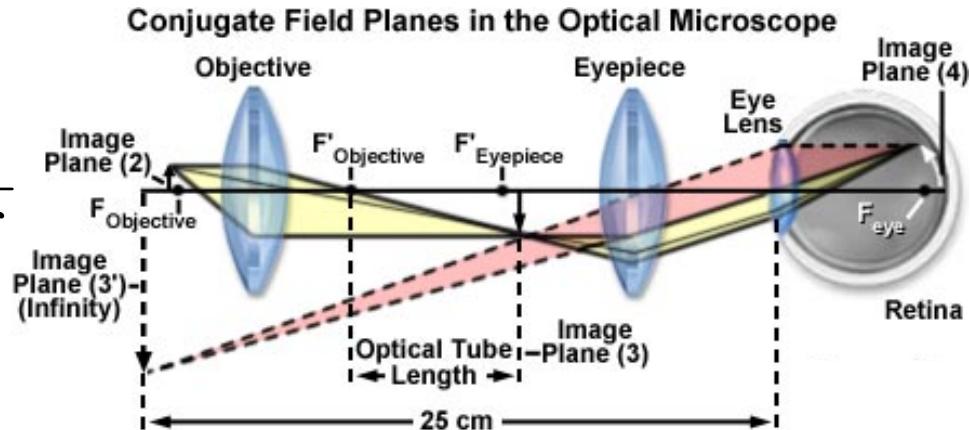
Light path in an optical imaging microscope



Images are from <http://micro.magnet.fsu.edu/>

Image formation

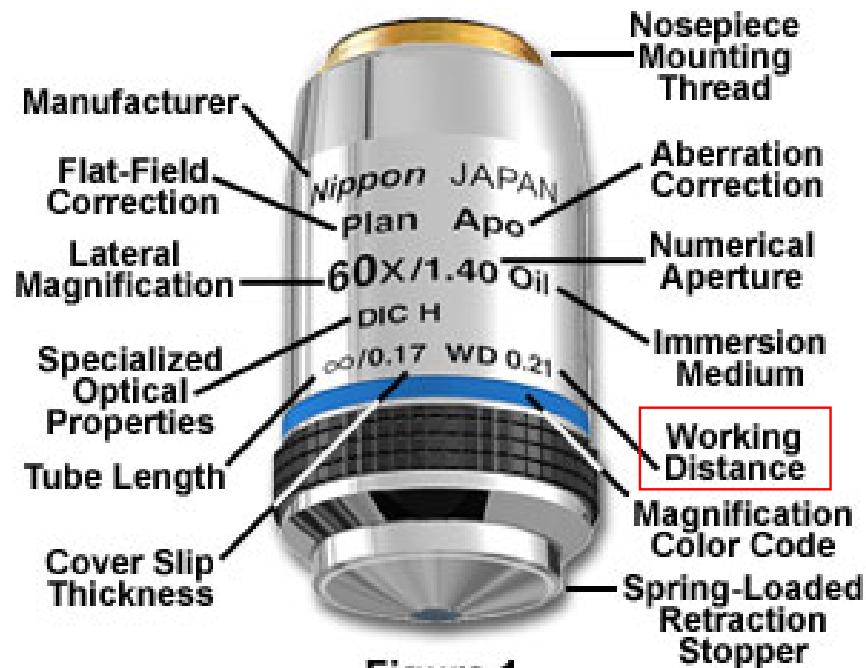
$$\frac{1}{d_o} + \frac{1}{d_i} = \frac{1}{f}$$



Images are from <http://micro.magnet.fsu.edu/>

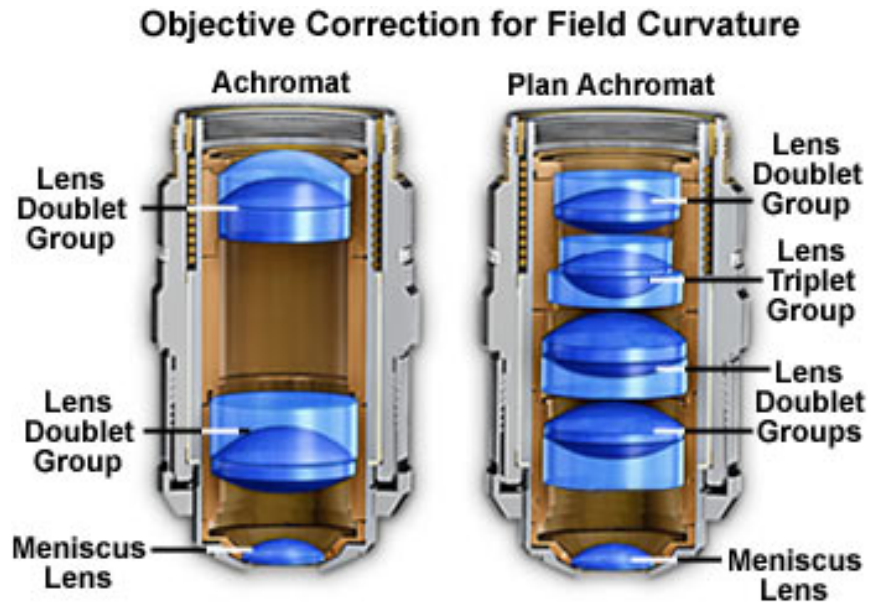
Specifications of an objective

60x Plan Apochromat Objective



Images are from <http://micro.magnet.fsu.edu/>

Achromatic



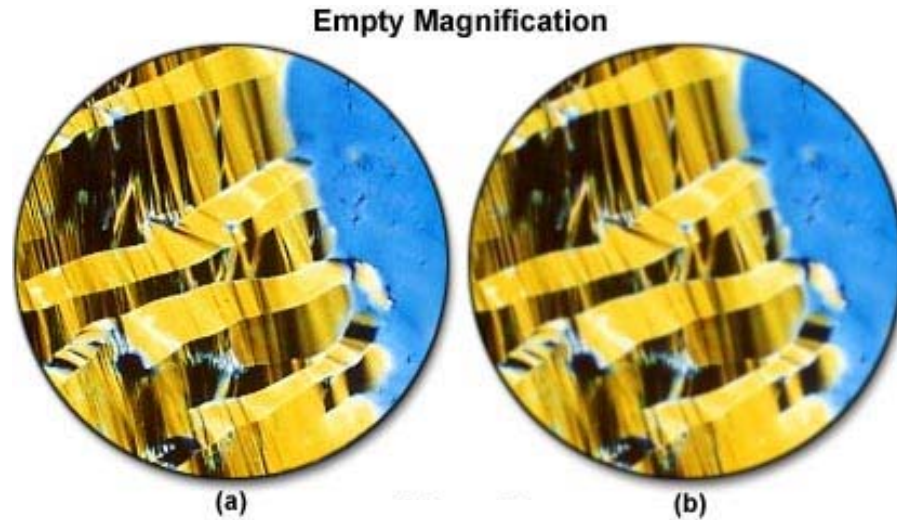
Images are from <http://micro.magnet.fsu.edu/>

Types of objectives

| Objective Type | Spherical Aberration | Chromatic Aberration | Field Curvature |
|------------------------|-----------------------------|-----------------------------|------------------------|
| Achromat | 1 Color | 2 Colors | No |
| Plan Achromat | 1 Color | 2 Colors | Yes |
| Fluorite | 2-3 Colors | 2-3 Colors | No |
| Plan Fluorite | 3-4 Colors | 2-4 Colors | Yes |
| Plan Apochromat | 3-4 Colors | 4-5 Colors | Yes |

Images are from <http://micro.magnet.fsu.edu/>

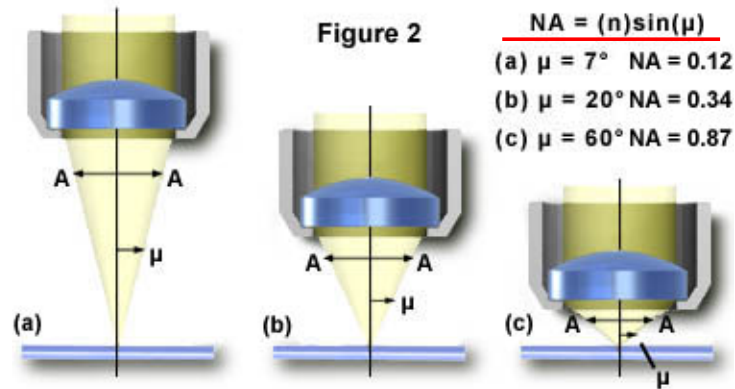
Resolution



Without **resolution**, magnified images cannot provide detailed information.

Images are from <http://micro.magnet.fsu.edu/>

Numerical aperture



Numerical Aperture and Airy Disc Size

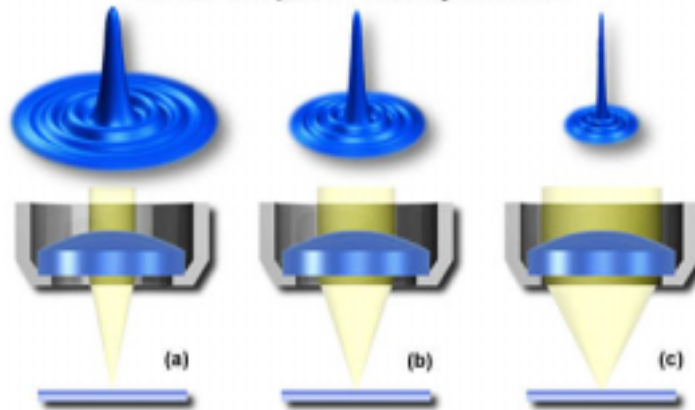


Figure 4

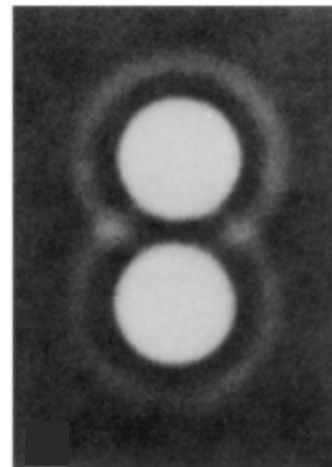
Images are from <http://micro.magnet.fsu.edu/>

Numerical aperture and resolution

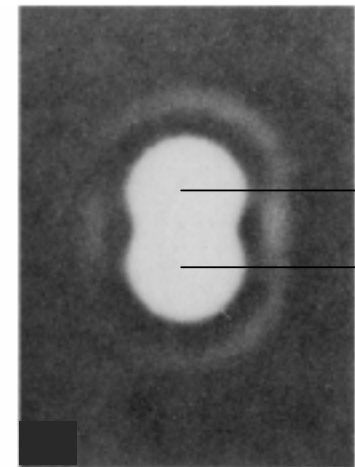
Rayleigh criterion:

resolution $\sim 0.61\lambda / \text{NA}$

For dry samples, $\text{NA} < 1.0$



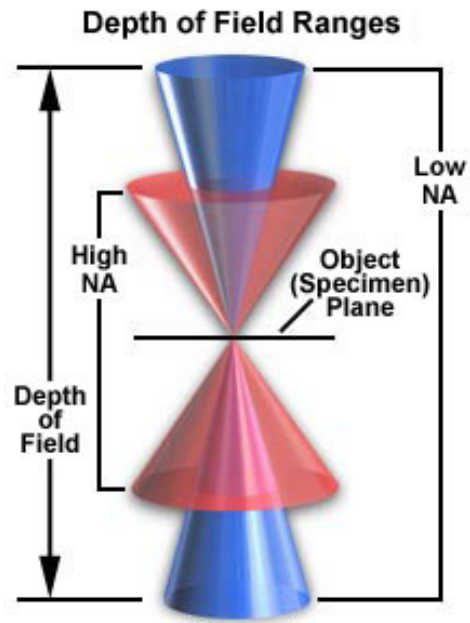
clearly resolved



resolution limit

Ref: M. Born and E.Wolf, *Principles of Optics*, 6th ed. (Pergamon, Oxford, 1980), Chap. 8.

Depth of field



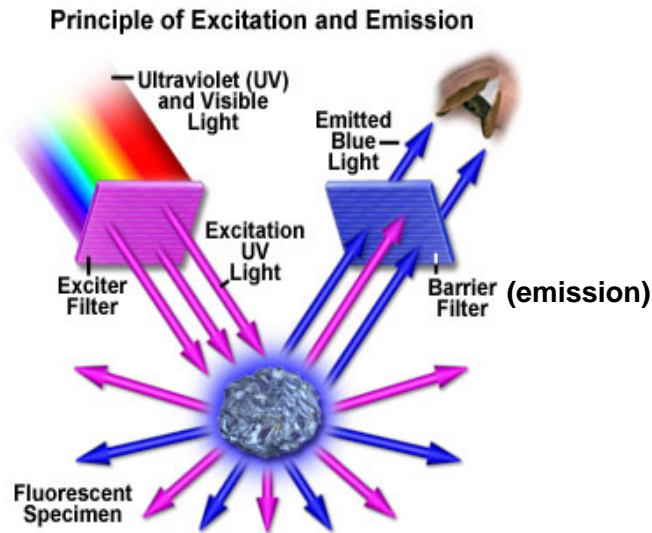
$$d = \lambda n / (\text{NA})^2$$

Images are from <http://micro.magnet.fsu.edu/>

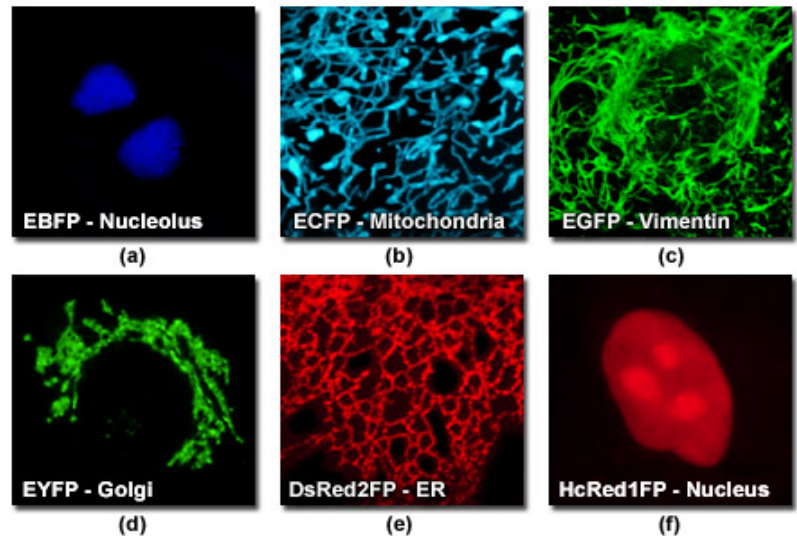
Contrast

Fluorescence microscopy

False color images. Usually a **monochrome** camera is used to capture the images, and color is added in the digital image files.

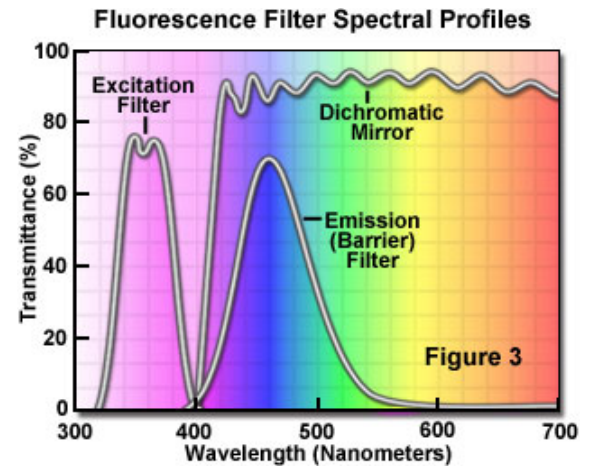
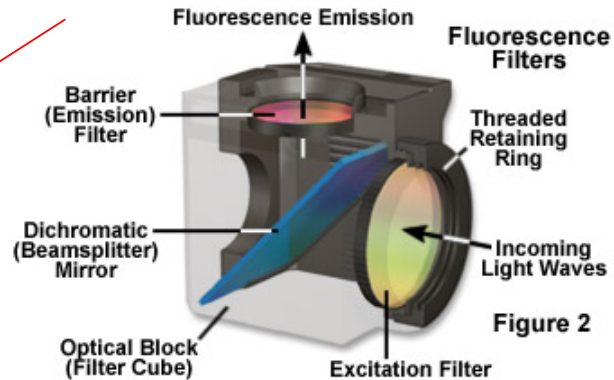
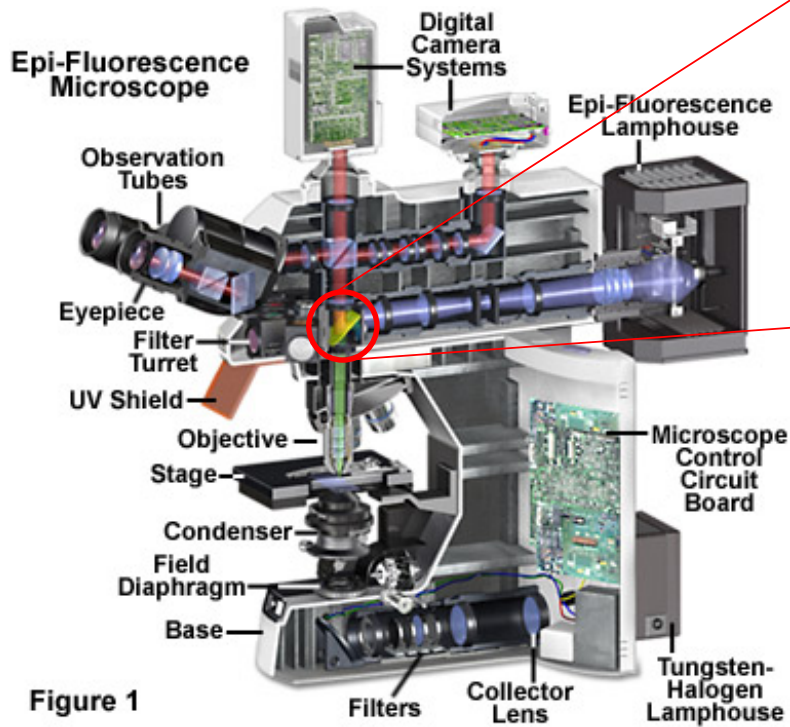


Digital Imaging of Localized Fluorescent Protein Chimeras



Images are from <http://micro.magnet.fsu.edu/>

Fluorescence microscopy



Images are from <http://micro.magnet.fsu.edu/>

Differential interference contrast (DIC)

Differential Interference Contrast Schematic

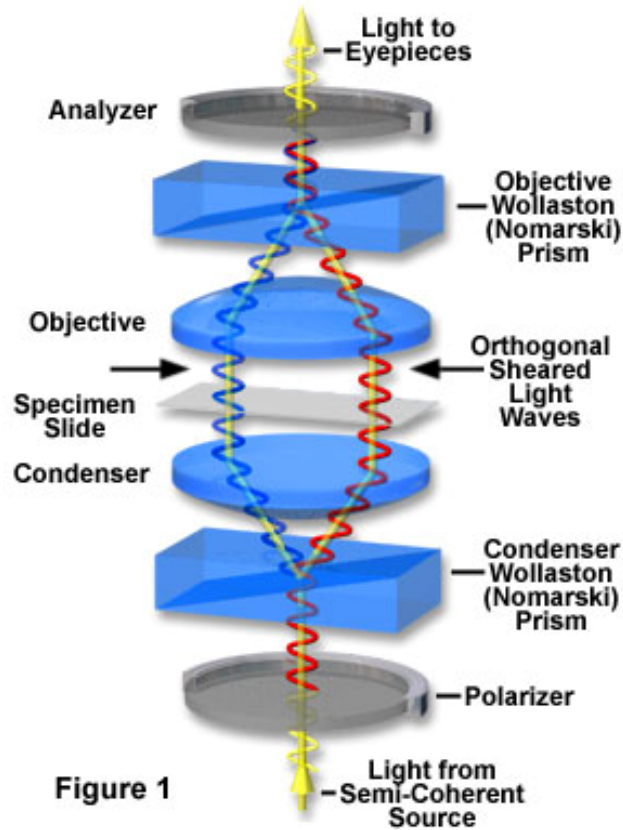
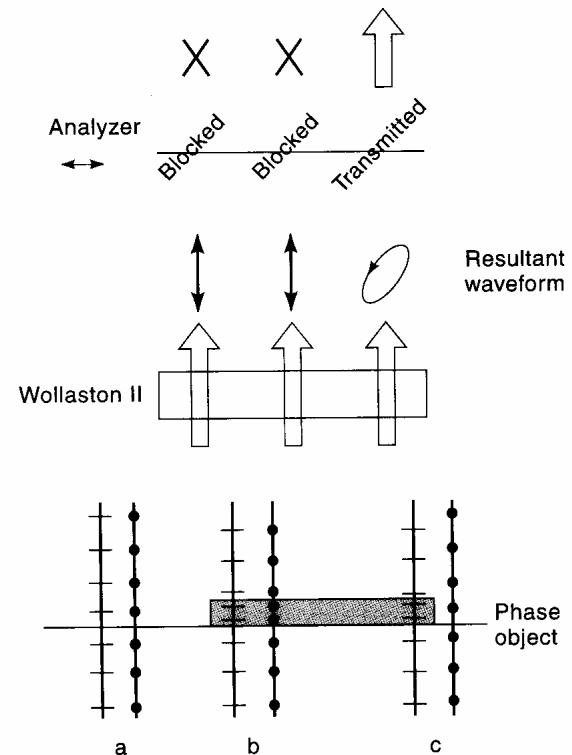


Figure 1

The contrast is from the **gradient** of the optical paths, not the optical paths.



Orientation in DIC

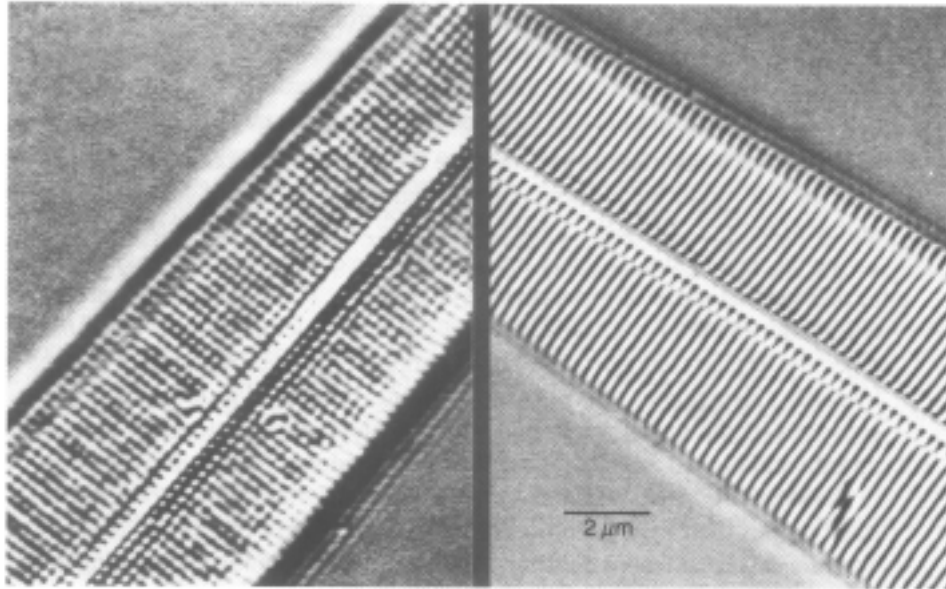


Figure 10-8

Effect of specimen orientation in DIC microscopy. Since the shear axis is fixed in DIC optics, the specimen itself must be rotated to highlight different features. Notice the differential emphasis of pores and striae in the shell of a diatom, *Amphipleura*, using video-enhanced DIC optics.

Comparison between phase contrast and DIC

Transparent Specimens in Phase Contrast and DIC

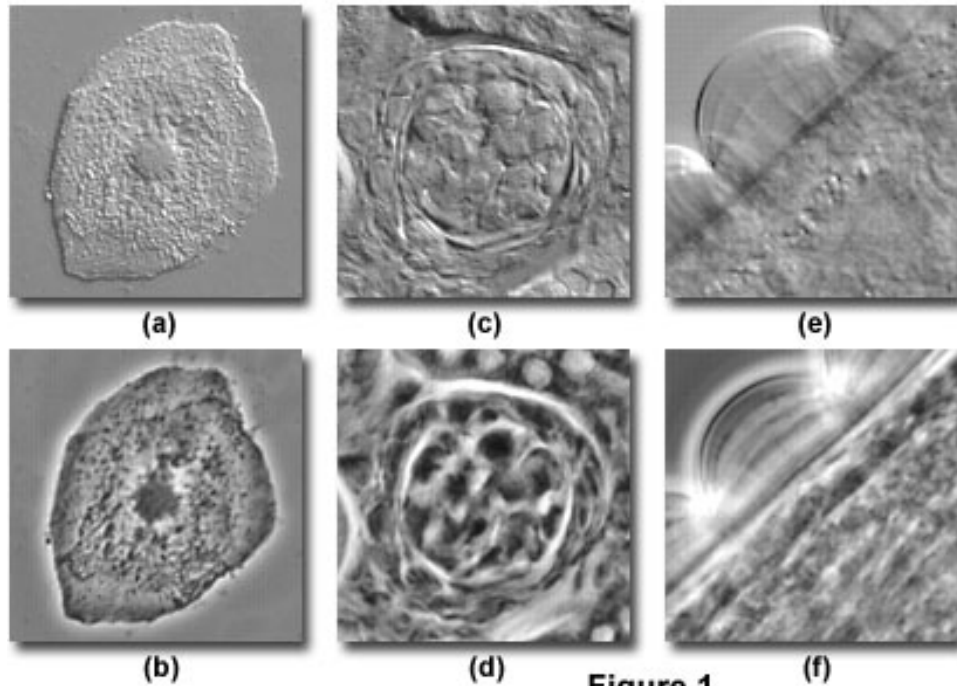
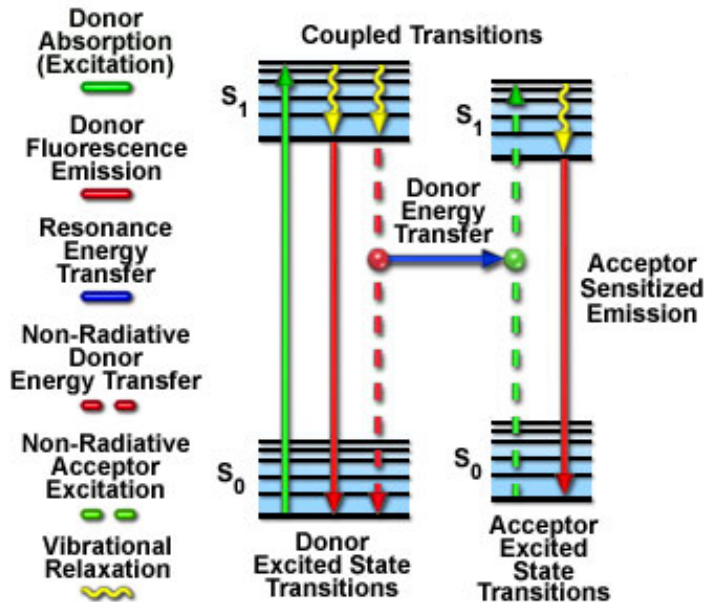


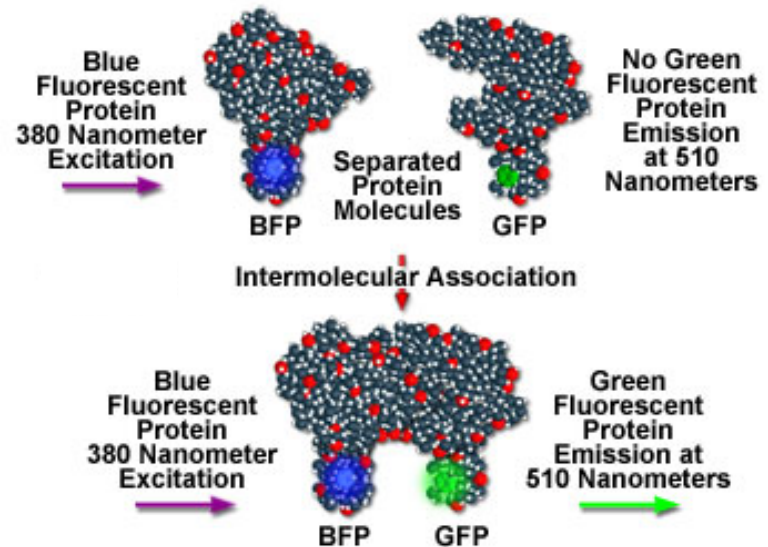
Figure 1

Fluorescence resonance energy transfer (FRET) Microscopy

Resonance Energy Transfer Jablonski Diagram



FRET Detection of *in vivo* Protein-Protein Interactions



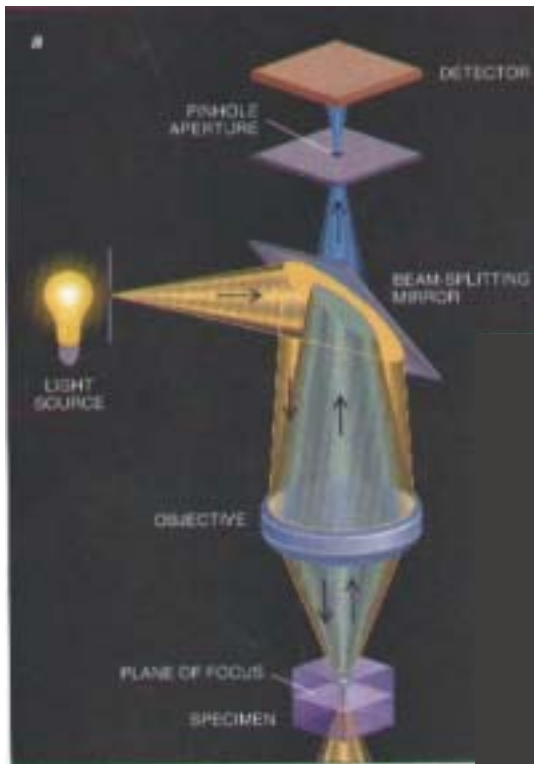
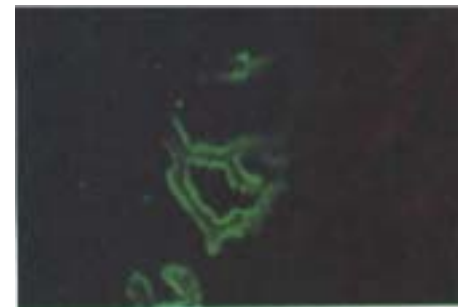
Confocal Microscopy

Confocal microscopy

Conventional fluorescence microscopy



Confocal microscopy



Confocal images

Improved depth resolution

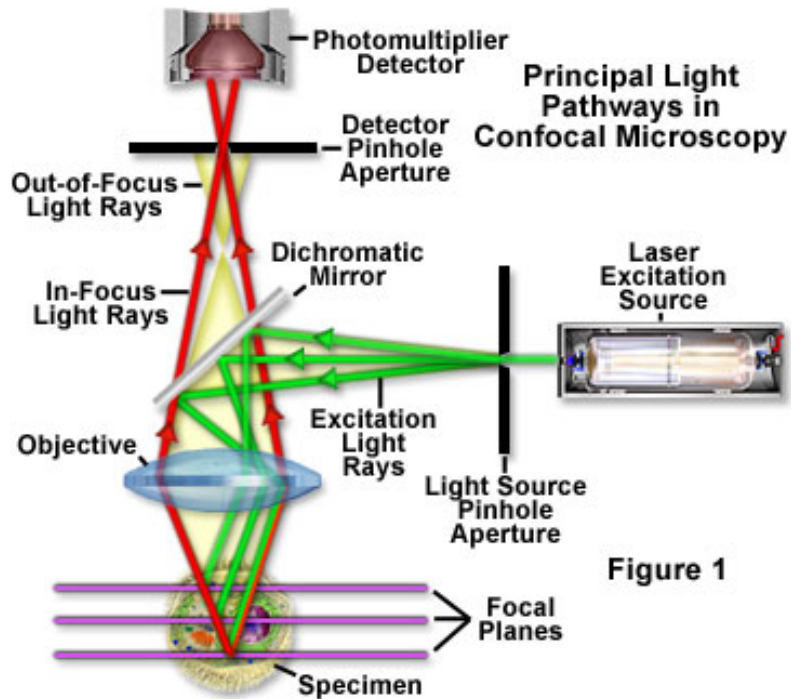
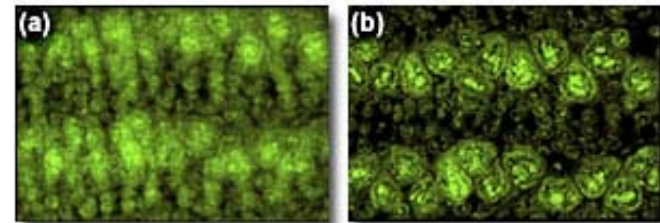
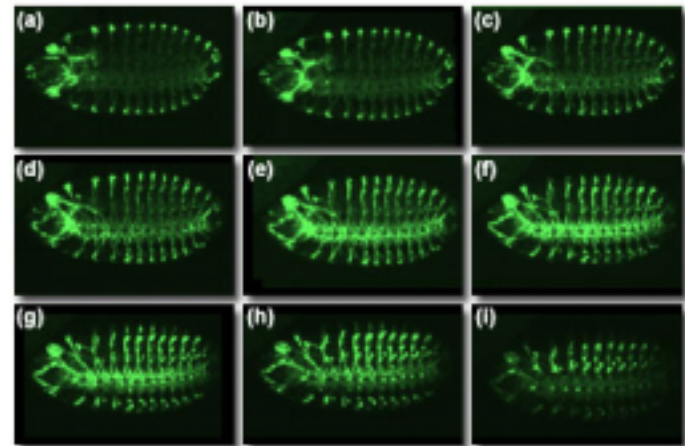


Figure 1

Butterfly Wing Epithelium

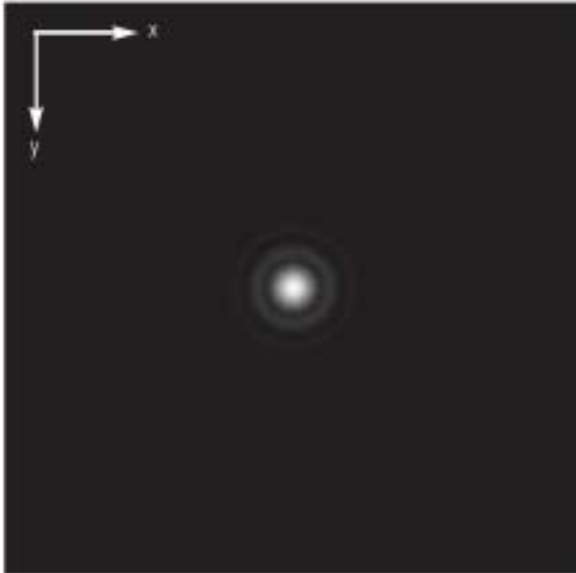


Optical Section Z-Series



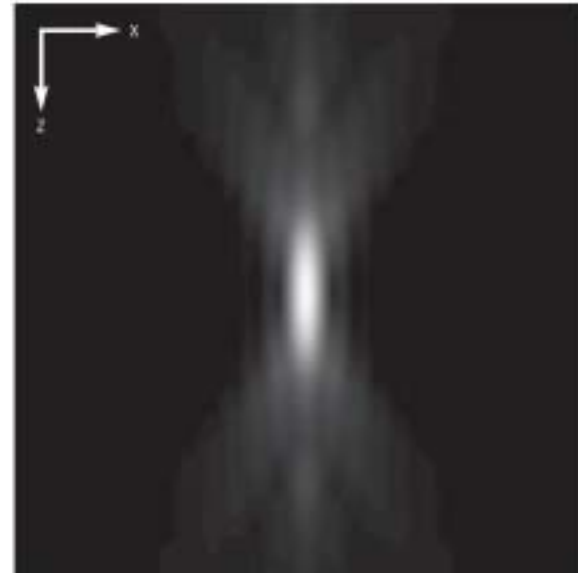
Images are from <http://micro.magnet.fsu.edu/>

Three-dimensional point-spread function



Lateral:

$$FWHM_{ill,lateral} = 0.51 \frac{\lambda_{exc}}{NA}$$

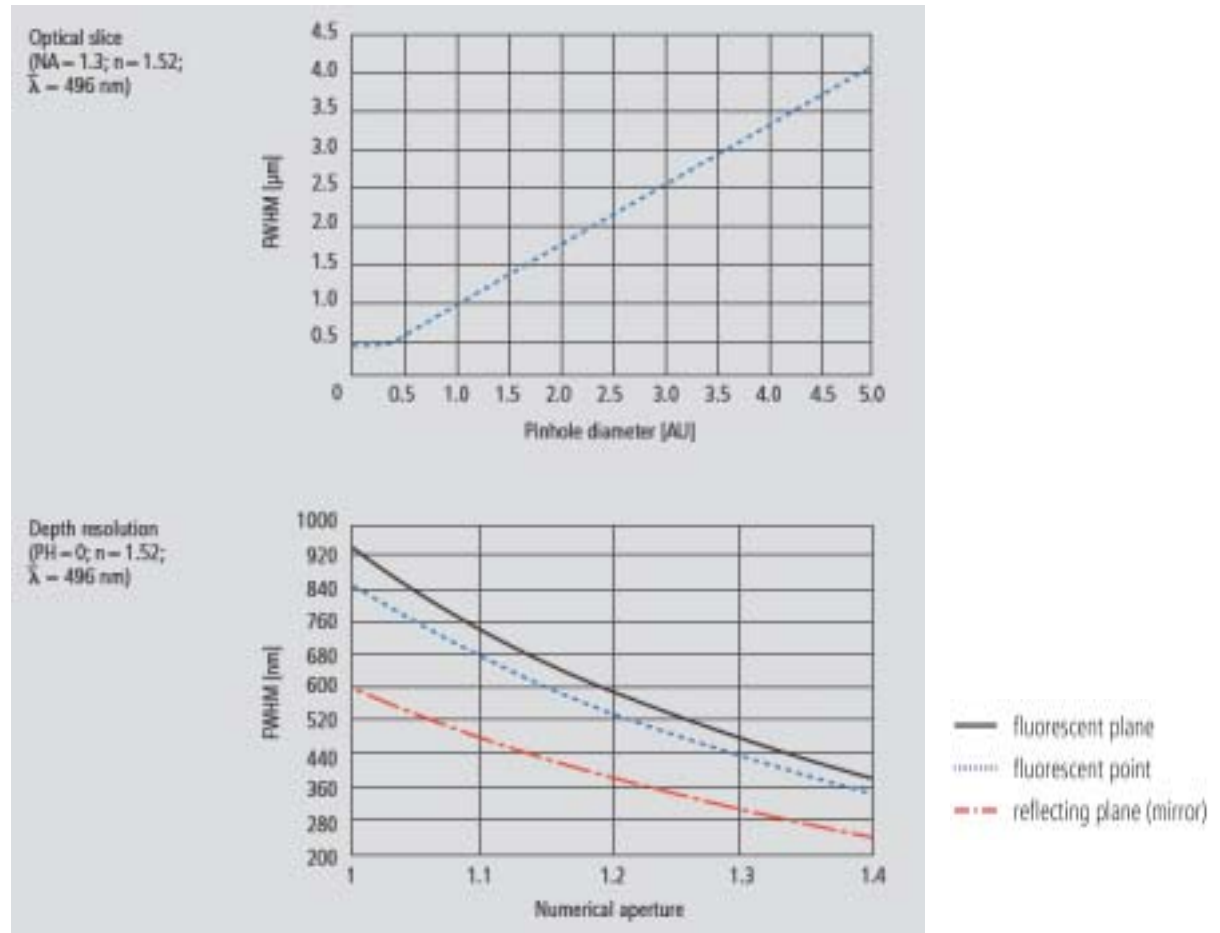


Axial:

$$FWHM_{ill,axial} = \frac{0.88 \cdot \lambda_{exc}}{(n - \sqrt{n^2 - NA^2})}$$

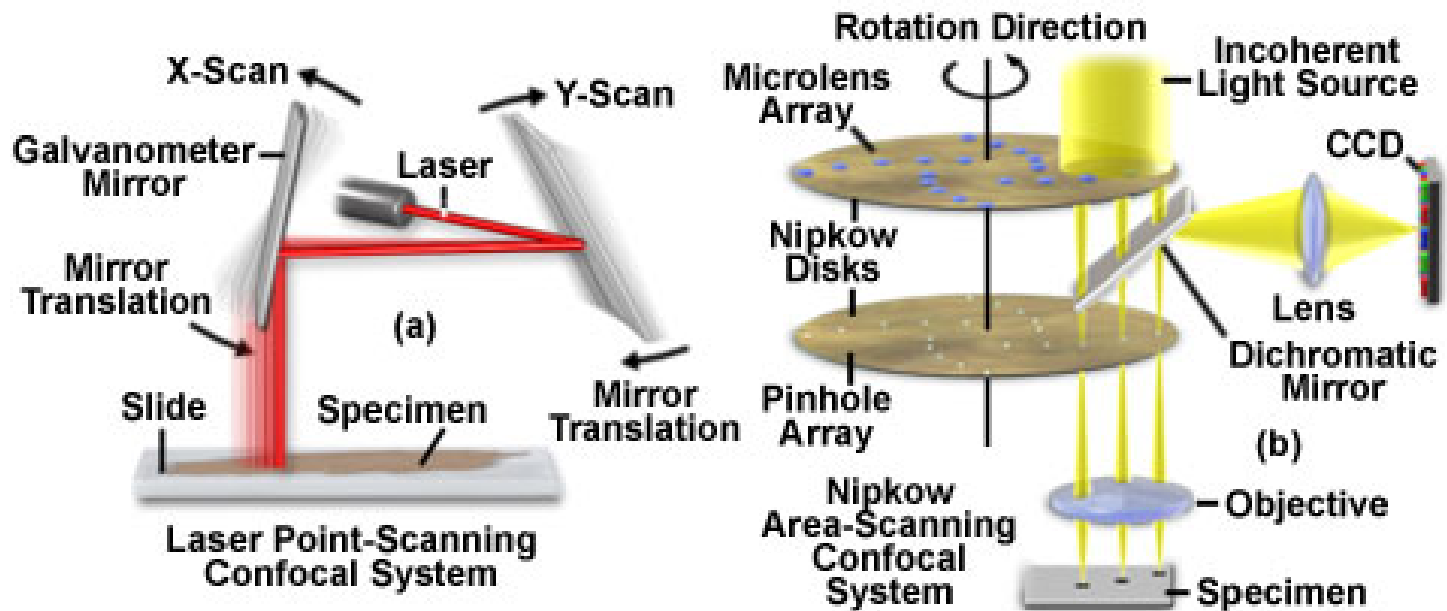
n = refractive index of immersion liquid,
 NA = numerical aperture of the microscope objective,
 λ_{exc} = wavelength of the excitation light

Effect of the pinhole diameter and NA



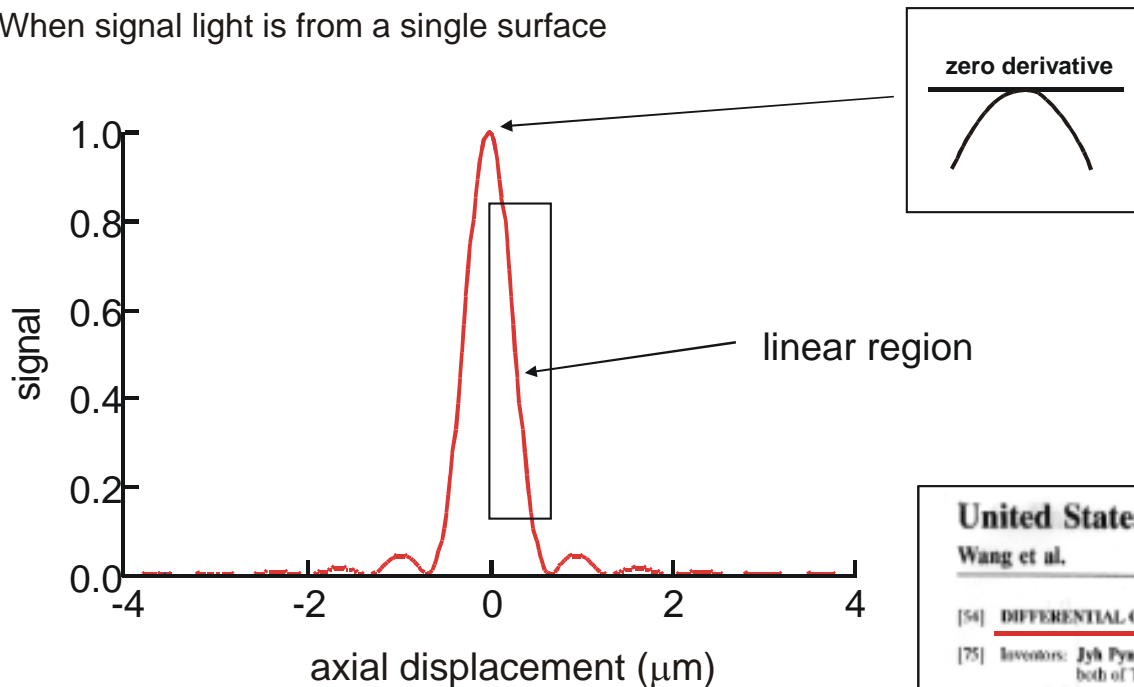
Scanning system

Point and Area-Scanning Confocal System Configurations



Nanometer depth resolution: differential confocal microscopy

When signal light is from a single surface



Typical slope in the linear region = $1/\mu\text{m}$

→ 10 nm displacement = 1% signal variation

United States Patent [19]

Wang et al.

[54] DIFFERENTIAL CONFOCAL MICROSCOPY

[75] Inventors: Jyh Pyng Wang; Chau-Hwang Lee,
both of Taipei, Taiwan

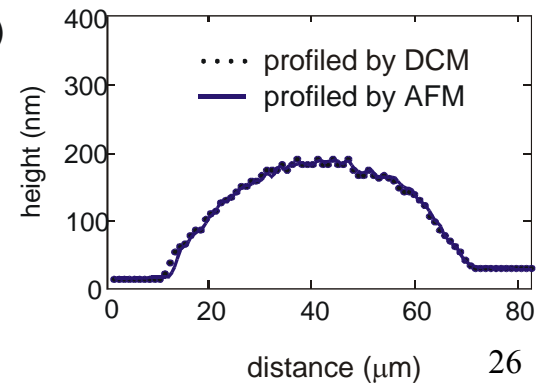
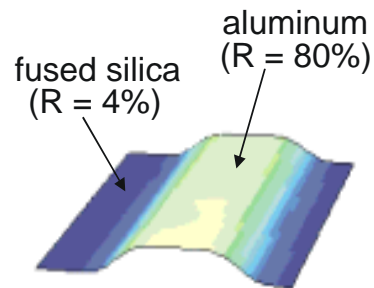
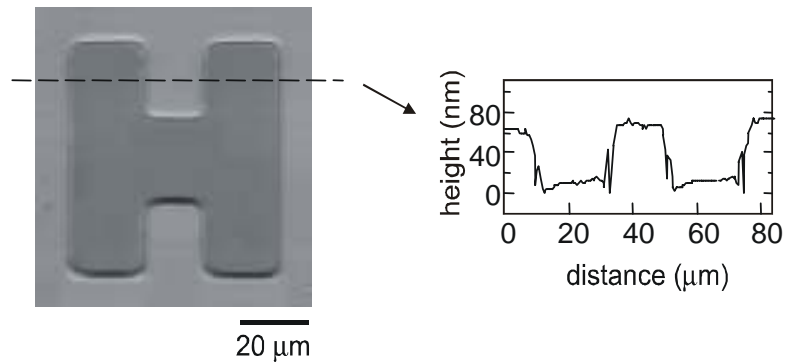
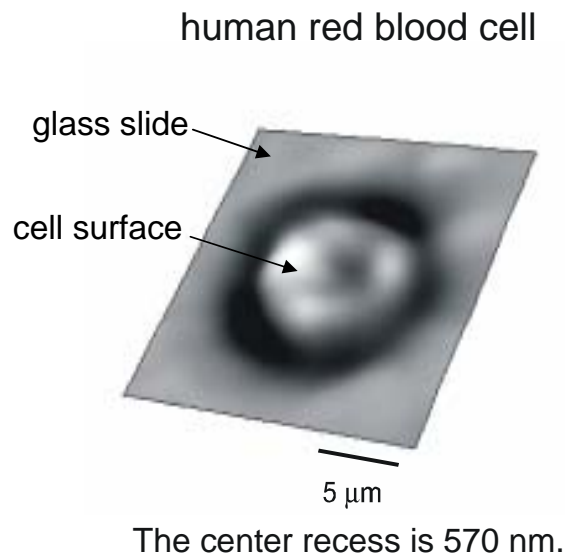
[73] Assignee: National Science Council of Republic
of China, Taipei, Taiwan

[21] Appl. No.: 889,647

[22] Filed: Jun. 8, 1996

Sample images of DCM

70-nm deep H-trench on InGaAs

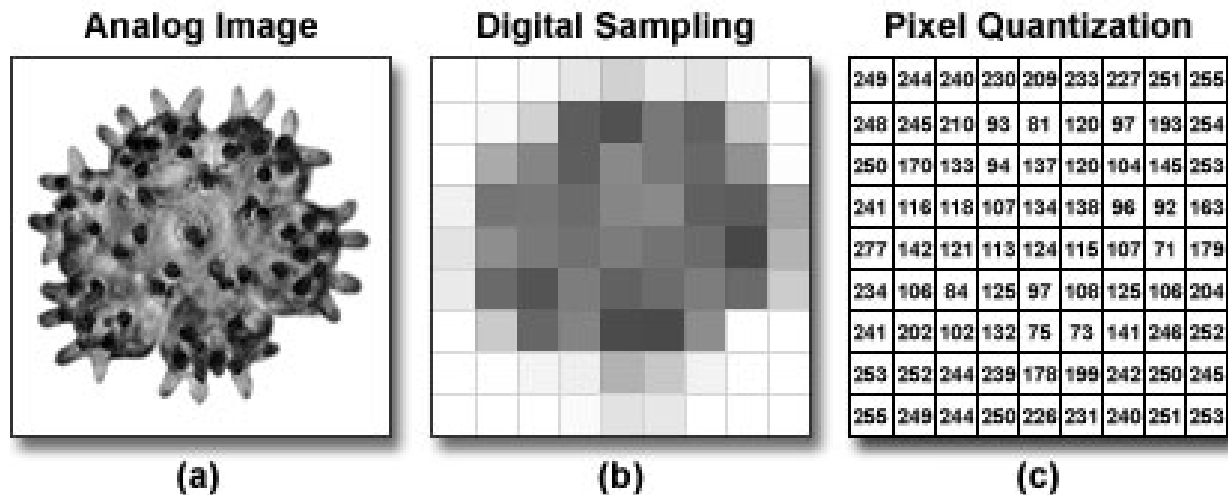


Ref: C.-W. Tsai, C.-H. Lee, and J. Wang, *Opt. Lett.* **24**, 1732 (1999).

Digital Images

A digitized image

Creation of a Digital Image

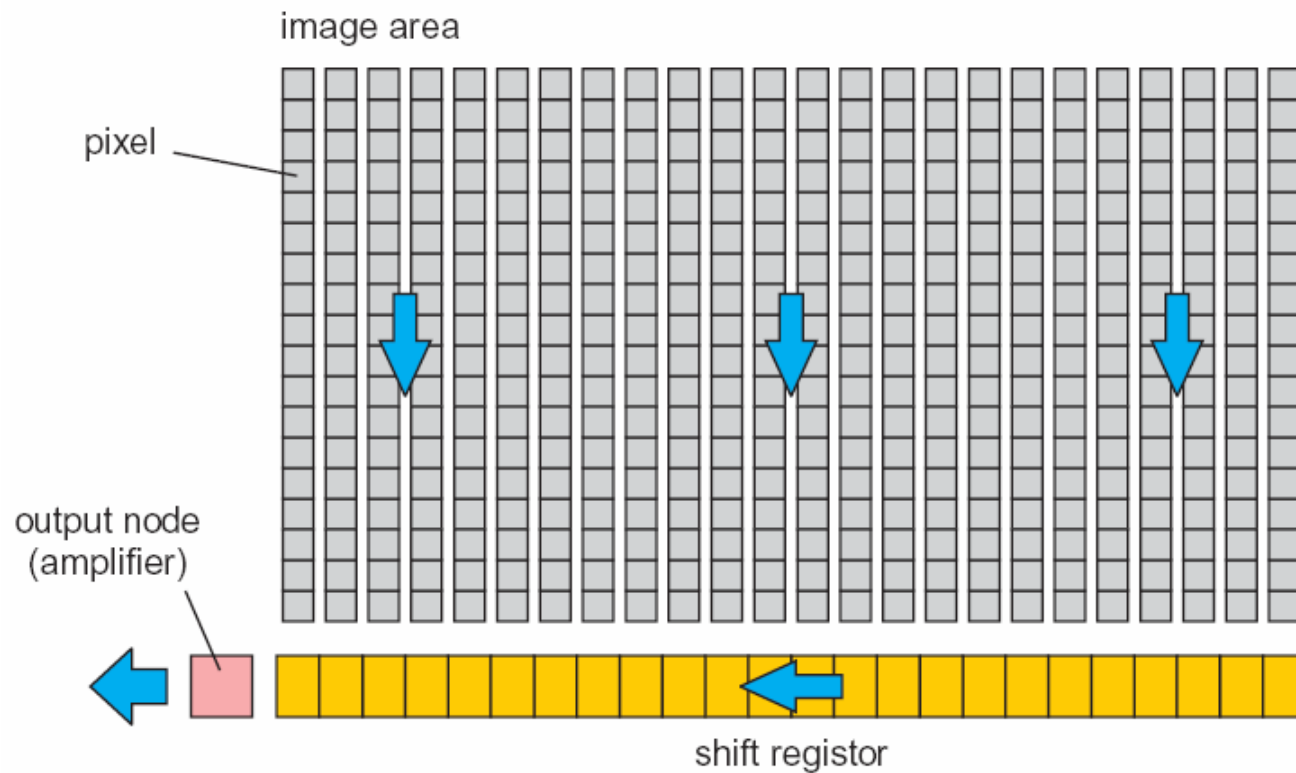


Images are from <http://micro.magnet.fsu.edu/>

Charge-coupled device (CCD)

2. CCD camera

exposure, readout, ADC resolution, and spatial resolution

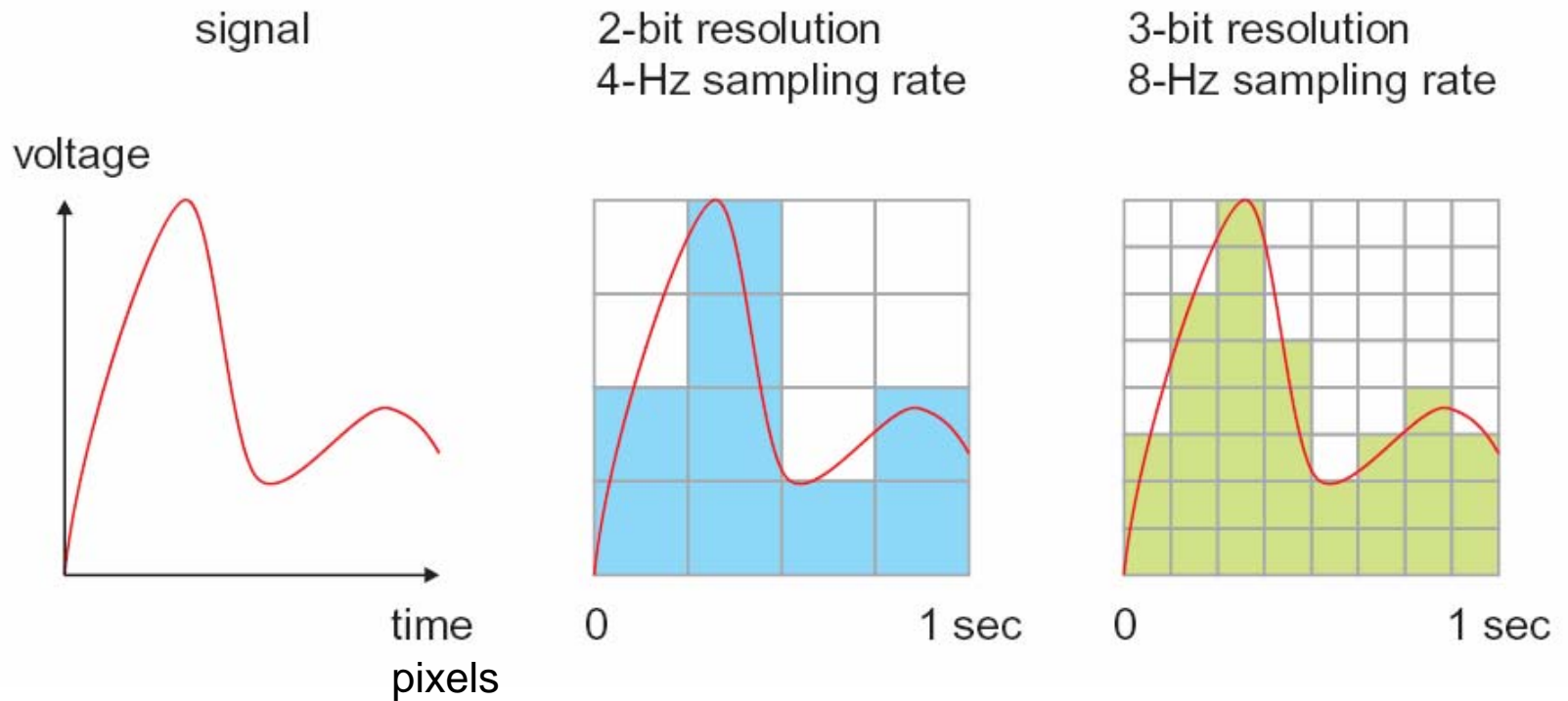


Specifications of CCD cameras

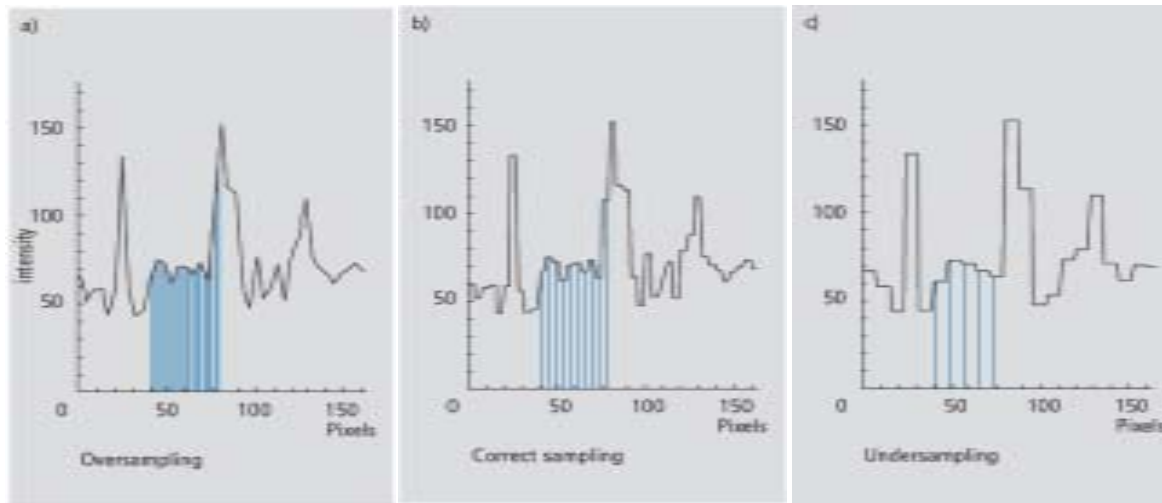
- pixel size ($8\text{ }\mu\text{m}$; $23\text{ }\mu\text{m}$)
- pixel resolution (640×480 ; 1024×1024)
- spectral response (300 nm to 1000 nm)
- well depth ($> 300,000\text{ e}^-$)
- dark current (50 pA/cm^2 at $20\text{ }^\circ\text{C}$)
- dynamic range ($> 85\text{ dB}$)
- digital or analog
- bit depth (10 bit; 12 bit; 14 bit...)



Signal digitization



Sufficient sampling



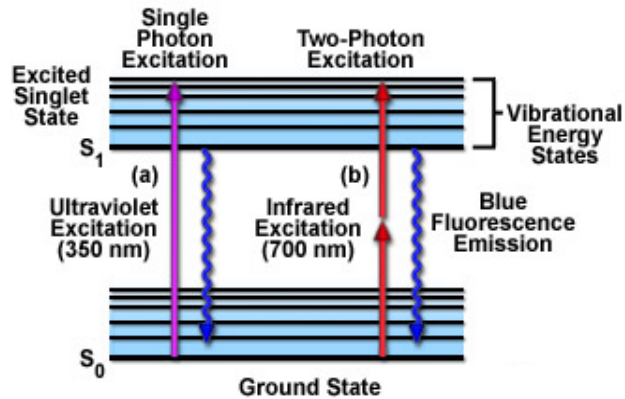
Sampling frequency $\geq 2 \times$ signal bandwidth

For CCD cameras, the pixel size on the image should be **smaller than half the optical resolution**.

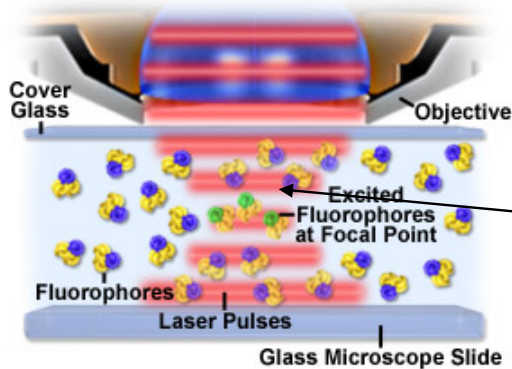
Related Technologies

Multiphoton Microscopy

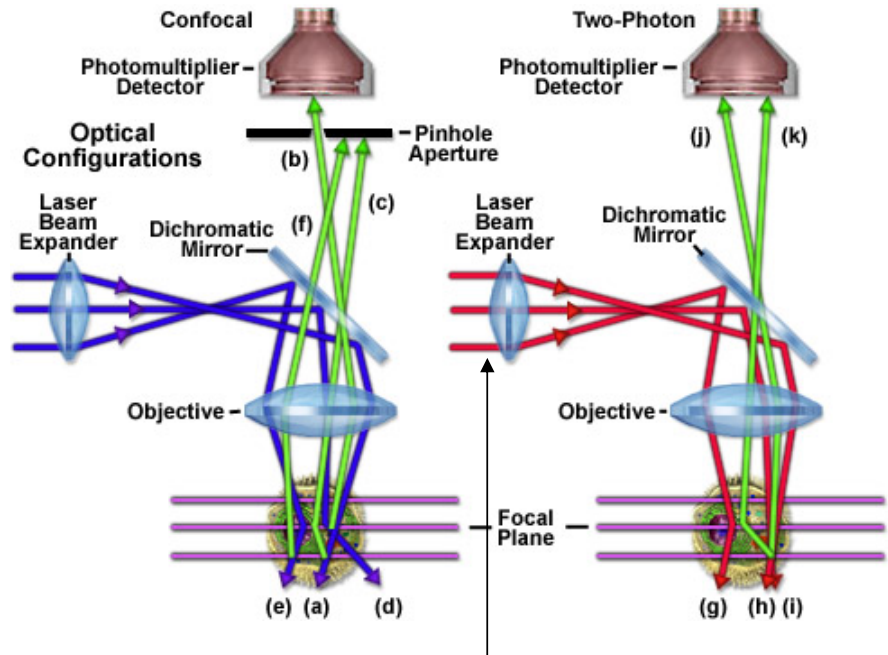
Two-Photon Jablonski Energy Diagram



Fluorophore Excitation in Multiphoton Microscopy

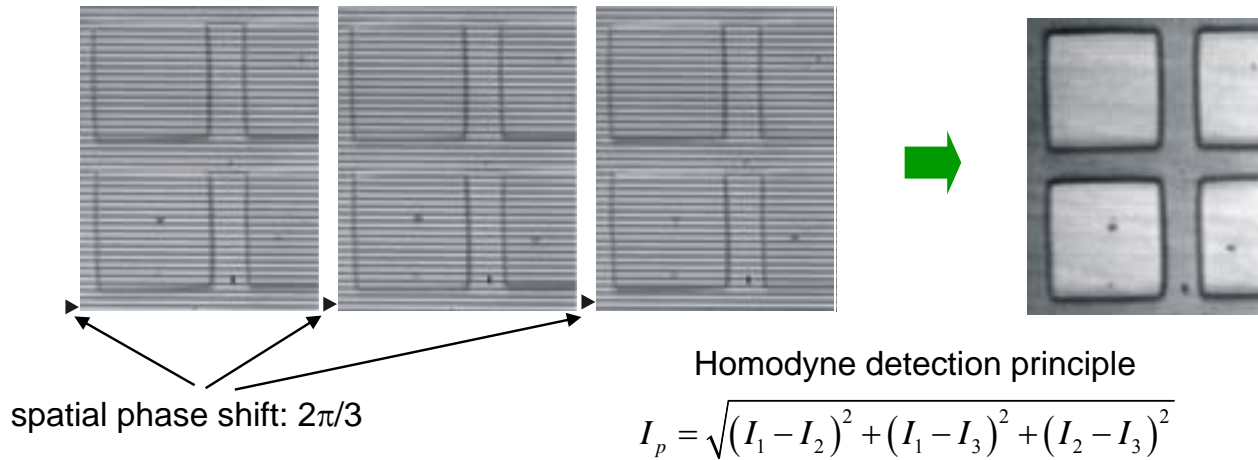


IR light can penetrate deeper into the tissues.

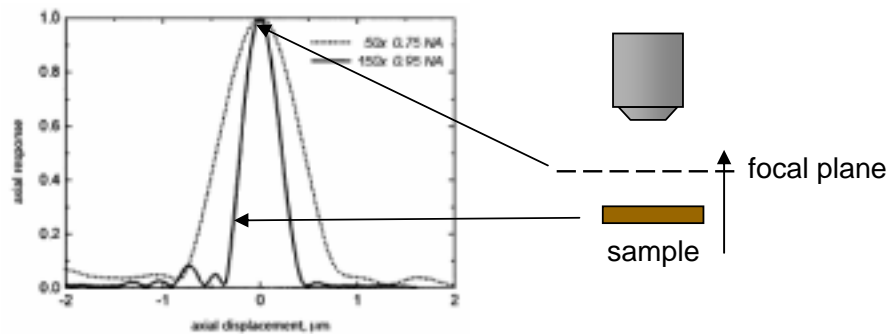


Femtosecond laser pulses are required to perform two-photon excitation.

Widefield optically sectioning microscopy



Axial response curve:



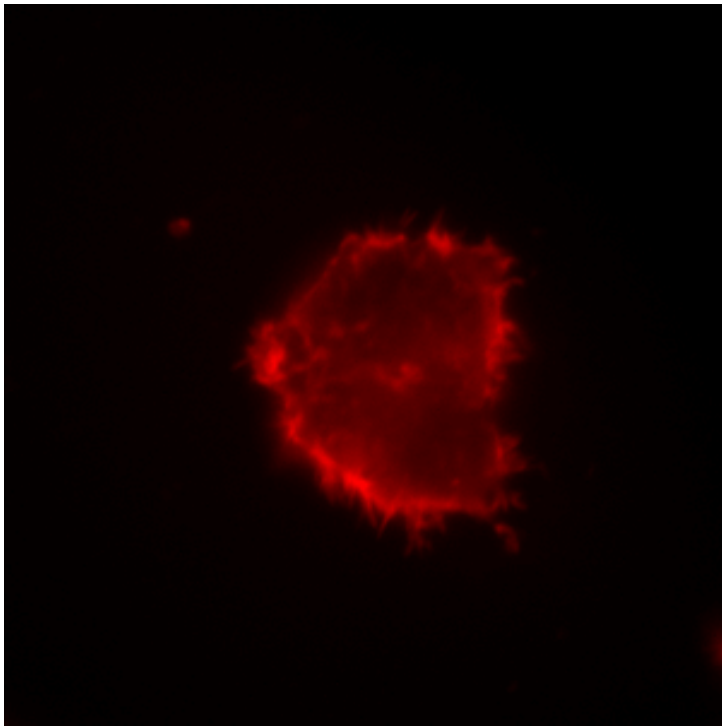
Ref: M. A. A. Neil, R. Juskaitis, and T. Wilson,
Optics Letters **22**, 1905 (1997).



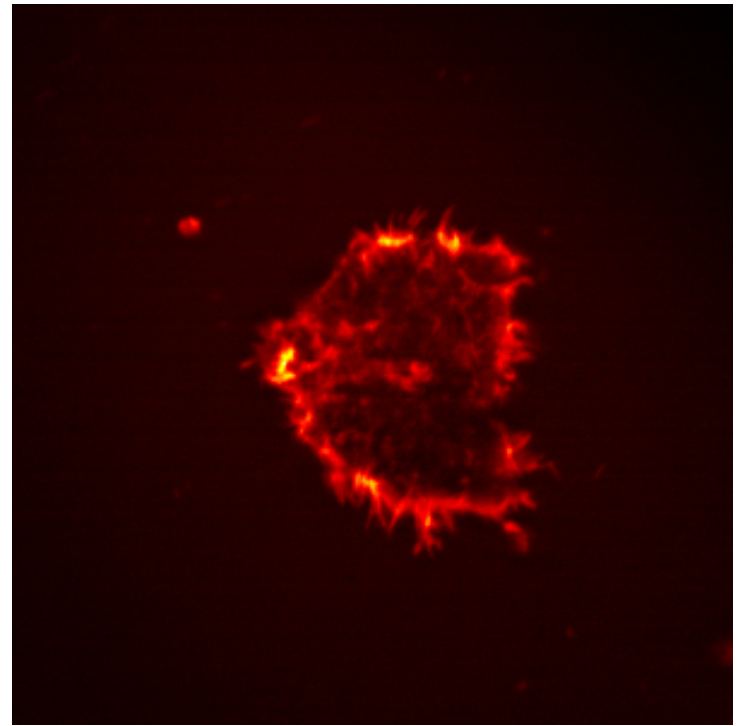
Carl Zeiss, ApoTome

Sectioned fluorescence images without scanning

Fluorescence

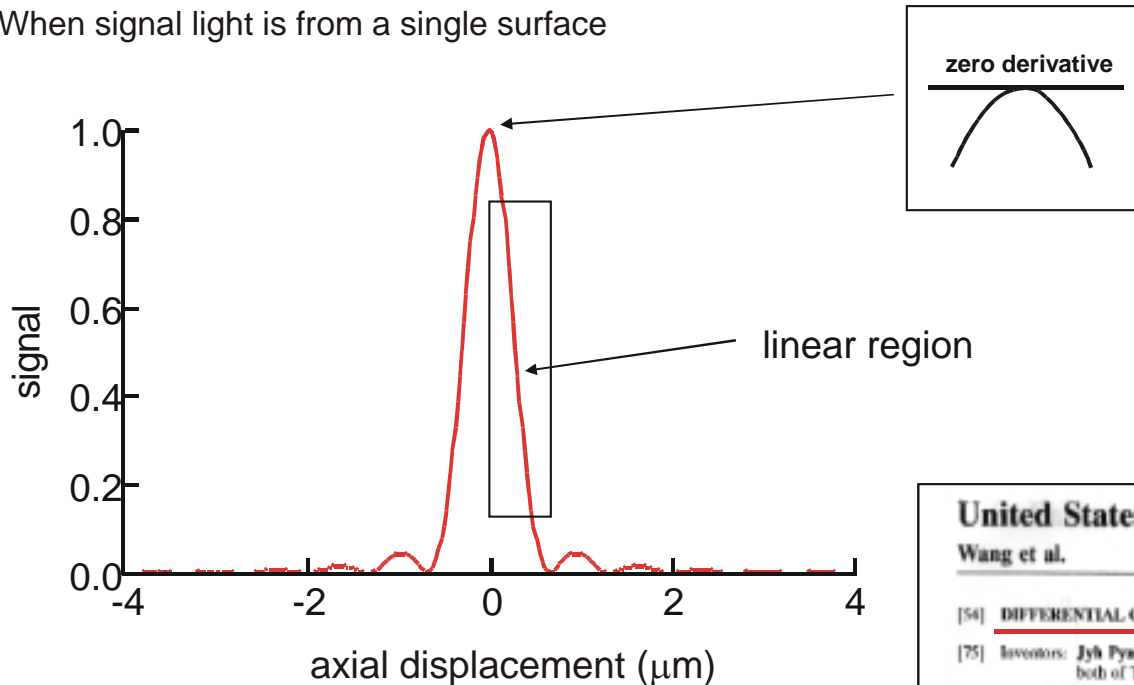


Optically sectioned



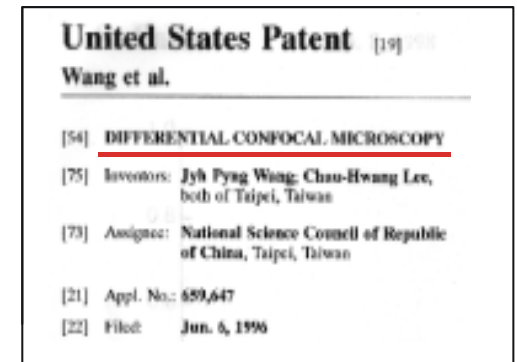
The concept of differential confocal microscopy

When signal light is from a single surface

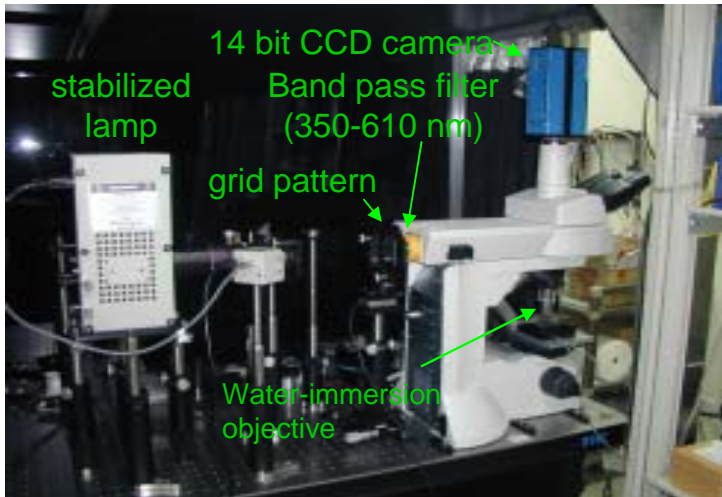


Typical slope in the linear region = $1/\mu\text{m}$

→ 10 nm displacement = 1% signal variation



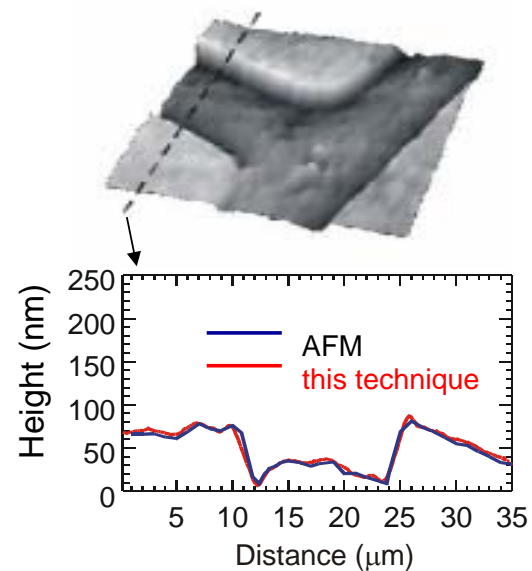
The NIWOP technique



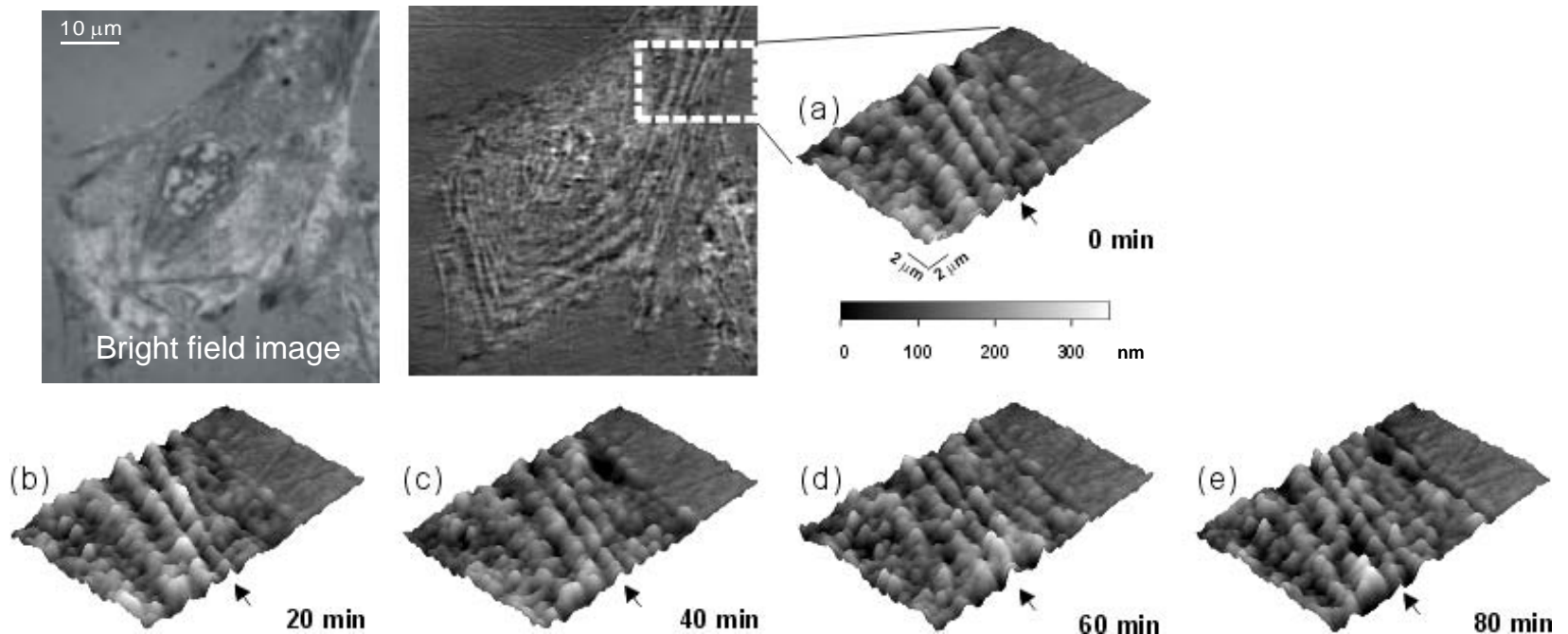
All the components are added
outside a bench-top microscope.

This technique is called **non-interferometric widefield optical profilometry** (NIWOP).

70 nm trench on InGaAs



Observation of membrane ripples of a living cell



The ripples are moving away from the cell edge with an average speed about $1.3\ \mu\text{m/h}$.

C.-C. Wang, J.-Y. Lin, and C.-H. Lee, *Optics Express* **13**, 10665 (2005).

Highlighted in *Virtual Journal for Biomedical Optics* (January 2006)

The Virtual Journal for Biomedical Optics

published by OSA

Exploring the interface of light and biomedicine

- Home
- Archives
- Search
- Subscribe
- Authors
- About
- OSA
- Login

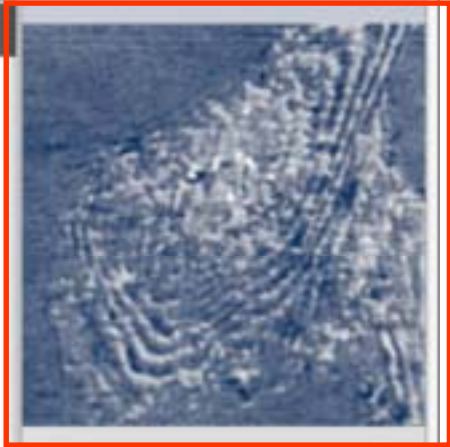
Editor-in-Chief: Gregory W. Faris • Vol. 1, Iss. 1 • January 17, 2006

- InfoBase Home
- ToC Alerts

Editorial

- Diffuse Imaging and Scattering
- Microscopy and Optical Coherence Tomography
- Optical Spectroscopies
- Image Reconstruction and Data Processing
- Biophotonics and Biosensors
- Optical Instrumentation and Endoscopy
- In Vitro Diagnostics and Histology
- Noninvasive Optical Diagnostics
- Vision and Color
- Novel Light Sources and Novel Optics
- Ocean and Plant Science
- Laser Eye Protection
- Biological Optical Materials

Editorial [\[show all papers in this category\]](#)



Membrane ripples on a living fibroblast cell measured using non-interferometric widefield optical profilometry. For details, see [Opt. Express 13, 10665 \(2005\)](#).

Stimulated emission depletion (STED) microscopy

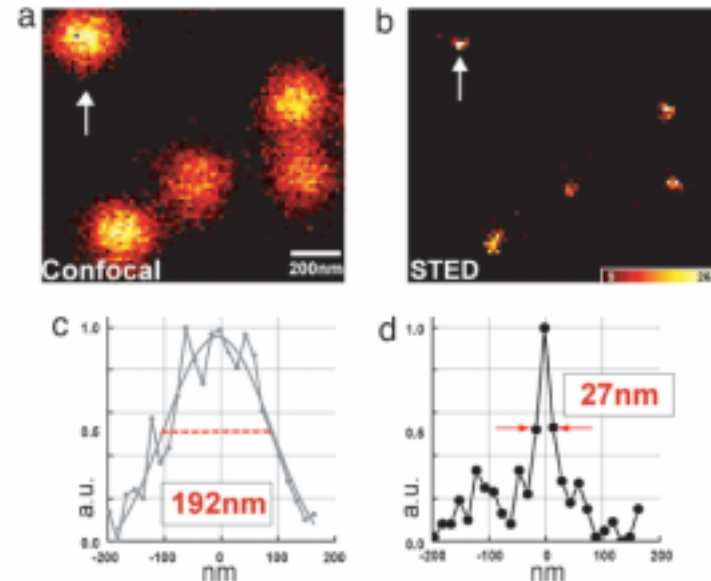
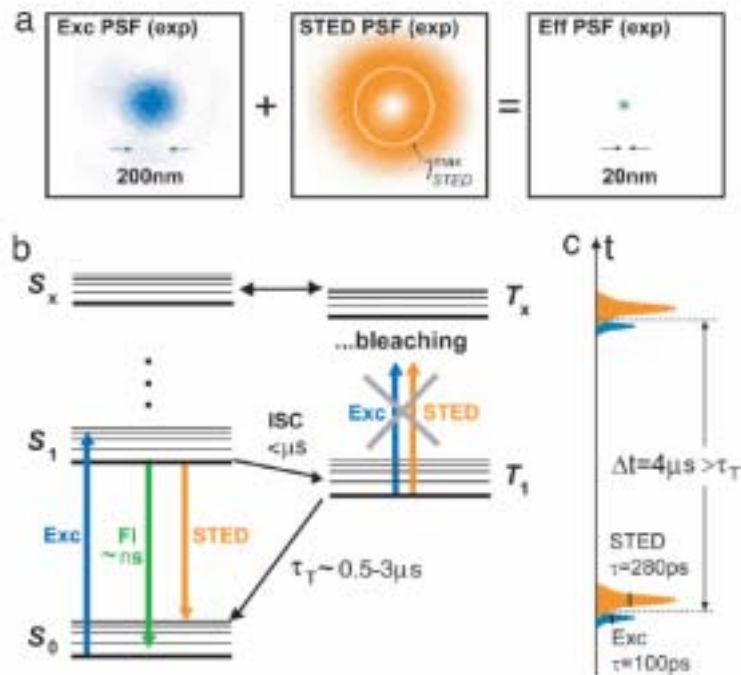
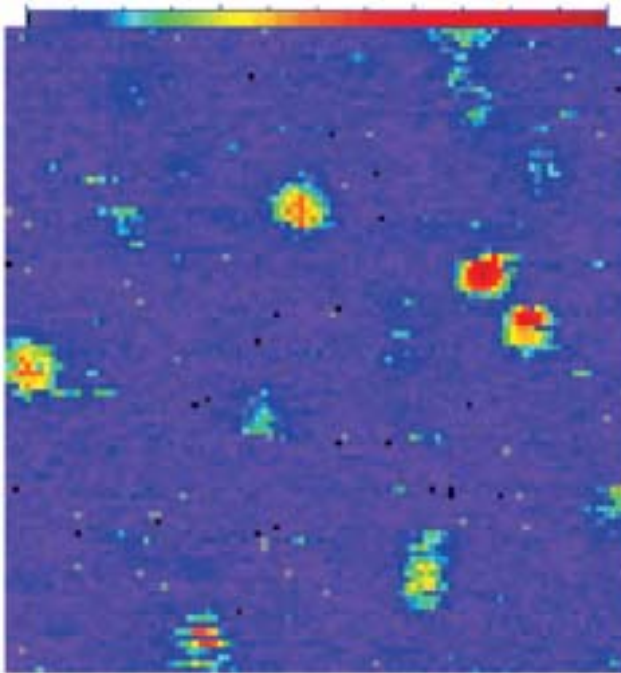


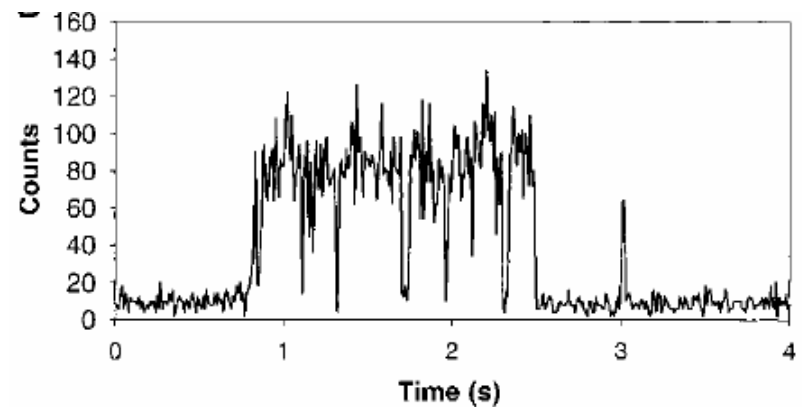
Fig. 3. Synaptotagmin I molecules form distinct spots on endosomes. (a and b) Whereas confocal microscopy exhibits a 190- to 200-nm diffraction-limited spot per endosome (a), STED microscopy recognizes sharp dots of 25–40 nm (b), both indicating its resolution as well as the punctated spatial arrangement of synaptotagmin I on the endosome. (c and d) Corresponding intensity profiles.

Ref: G. Donnert et al., *Proc. Natl. Acad. Sci. USA* **103**, 11440 (2006).

Confocal microscopy for single molecules



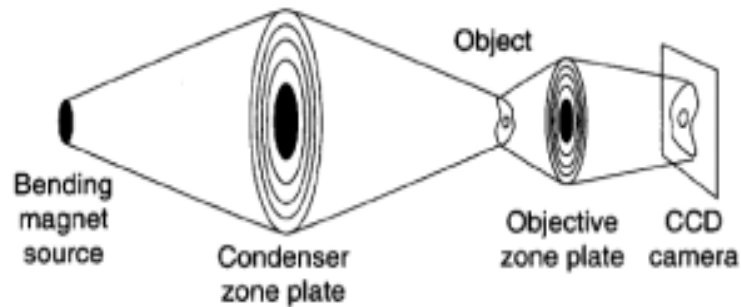
Blinking



Ref: W. E. Moerner and M. Orrit, *Science* **283**, 1670 (1999).

X-ray microscopy

(a) TXM: transmission x-ray microscope



(b) STXM: scanning transmission x-ray microscope



The resolution of a **zone plate** is almost equal to the smallest (outermost) zone width. With current e-beam lithography, the smallest zone width can be ~15 nm.

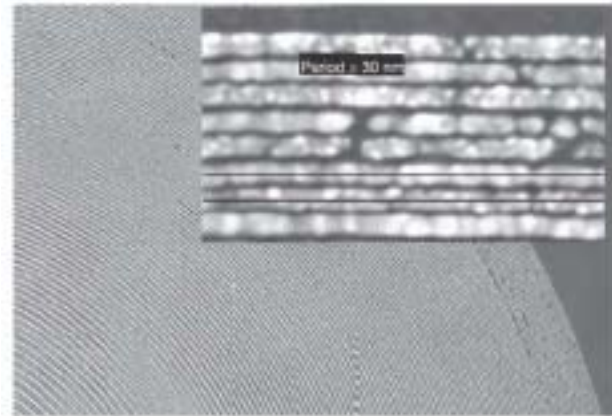


Figure 3 | Scanning electron micrograph of a zone plate with 15 nm outermost zone. Shown in the inset is a more detailed view of the outermost zones. The zonal period, as indicated by the two black lines, is measured to be 30 nm. The zone placement accuracy is measured to be 1.7 nm.

Ref: C. Jacobsen, *Trends Cell Biol.* **9**, 44 (1999).

Ref: W. Chao et al, *Nature* **435**, 1210 (2005).

Compact soft x-ray microscope

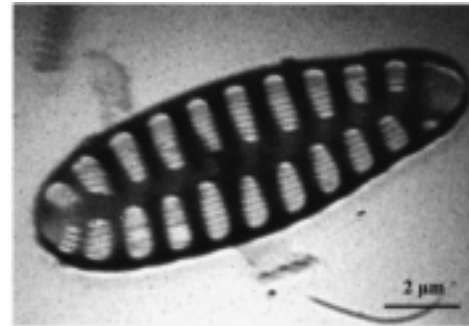
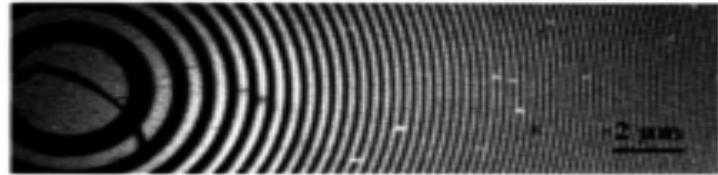
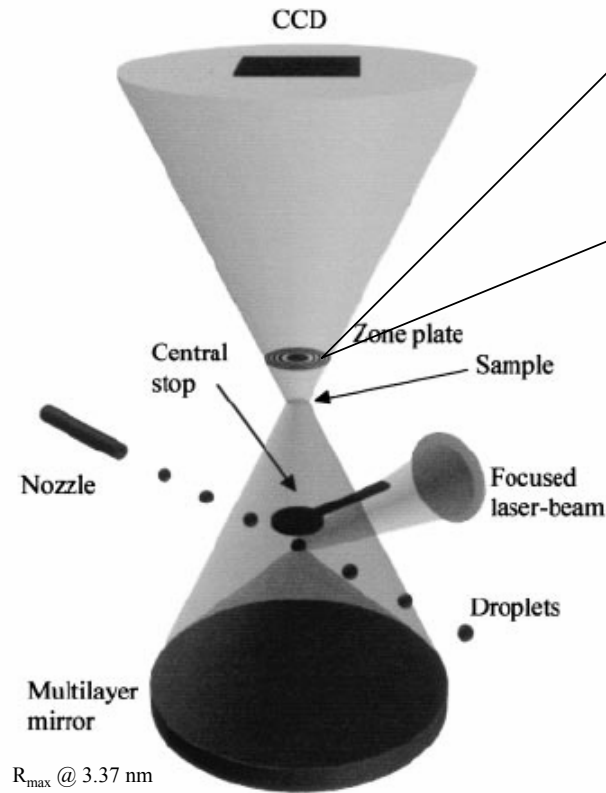
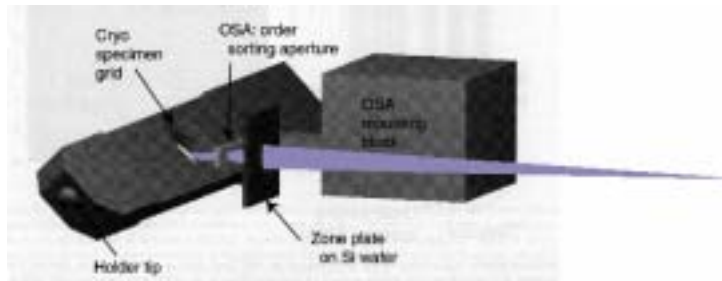


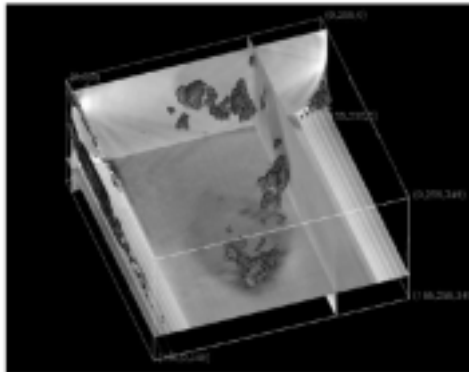
Image of diatom

Resolution ~ 100 nm

X-ray microtomography



Vesicles inside a cell



Resolution ~ 250 nm

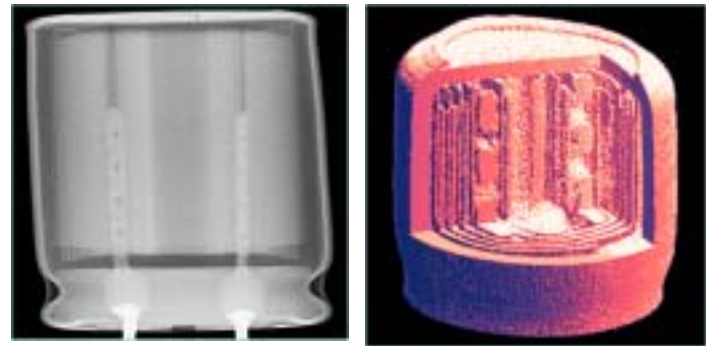
Ref: Y.Wang et al., *J. Microsc.* **197**, 80 (2000).

Commercial product available



<http://www.microphotonics.com>

Capacitor



Resolution < 10 μm